

Effect of γ -radiation on the ratio of [^{18}F]2-fluoro-2-deoxy-D-glucose to glucose utilization in human glioblastoma cells *in vitro*

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The glucose consumption in tumours *in vivo* as reflected by uptake of [^{18}F]2-fluoro-2-deoxy-D-glucose (^{18}FDG) using positron emission tomography (PET) is currently under investigation as a measure of tumour response to radiotherapy. The calculation of cerebral metabolic rate of glucose from ^{18}FDG -PET data requires a proportionality factor referred to as the lumped constant. In the present *in vitro* study, the utilizations of ^{18}FDG and glucose have been measured in a human glioblastoma cell line (86HG-39) as a function of γ -radiation dose with various post-irradiation times and of different fractionation modes. The ratio of utilization of ^{18}FDG to that of glucose ($R_{\text{F/G}}$), assumed to correspond to the lumped constant, was observed to increase 12 and 24 h after single fraction γ -exposure by factors ranging from 1.2 to 1.5 compared with the non-irradiated controls. It decreased after multiple fraction γ -exposure (4×2 Gy) by a factor of 0.7 compared with the single fraction schedule (1×8 Gy). The results suggest that the affinities of glucose transporters or hexokinase enzyme or both for ^{18}FDG and glucose could be influenced by γ -irradiation in this tumour cell line *in vitro*. Apparent changes of the glucose consumption determined with PET in human tumours following radiotherapy may, therefore, not be solely due to changes in cellular metabolism or cell number but may also be due to changes in $R_{\text{F/G}}$.

1. Introduction

An increased energy demand is a well recognized characteristic of most malignant tumours. Glucose is the major source of energy to living cells and cancerous cells are known to show enhanced consumption of glucose signifying the increased energy demand. The advent of novel *in vivo* imaging methods, such as positron emission tomography (PET), and the concomitant development of appropriate mathematical models (Sokoloff *et al* 1977) have enabled the determination of the glucose metabolic rate for the human brain. The *in vivo* calculation of tumour glucose metabolic rate by PET using [^{18}F]2-fluoro-2-deoxy-D-glucose (^{18}FDG) may be of value in predicting the clinical response of tumours to radiotherapy and chemotherapy.

The model which has been developed by Sokoloff *et al* (1977) for *in vivo* quantification of cerebral glucose metabolic rate in rats is based upon the assumption that the utilization of FDG during a limited time of less than 1 h is proportional to that of glucose. For normal human subjects Lucignani *et al* (1993) have found the optimal time between 60 and 120 min. No conclusive estimate is available for tumours. For an *in vitro* model, where equilibration is attained faster than a complex *in vivo* system, a 45 min period for irreversible entrapment of deoxyglucose-6-phosphate in cells may be reasonable (Sokoloff *et al* 1977; Herholz *et al* 1990; Som *et al* 1980). It is further assumed that the utilization of glucose and ^{18}FDG reach and maintain steady state during this period (Sokoloff *et al* 1977). This was experimentally verified *in vivo* (Reivich *et al* 1985). The lumped constant

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(LC) in Sokoloff's model represents the relation between the kinetics of ^{18}F FDG to those of glucose (Herholz *et al* 1990; Gjedde *et al* 1985). Since the LC is reported to change under pathological conditions (Gjedde *et al* 1985), it may also be affected by therapeutic interventions, such as radiotherapy or chemotherapy. The *in vivo* measurement of changes of the LC after therapeutic interventions is rather difficult. In this study, an *in vitro* model for determination of changes of the ratio between ^{18}F FDG and glucose utilizations ($R_{\text{F/G}}$) under steady state conditions has been developed assuming that this ratio corresponds to the LC *in vivo*. Using the *in vitro* model, radiation induced changes on the $R_{\text{F/G}}$ has been measured. The *in vitro* study determines the $R_{\text{F/G}}$ as a function of the γ -radiation dose at various post-irradiation times and of different modes of irradiation in monolayers of a human glioblastoma cell line.

2. Materials and methods

2.1 Cell culture

Human glioblastoma (HG) cells, 86HG-39, were cultured as monolayer in Leighton tubes (NUNC, Denmark). Approximately 0.3×10^6 cells were seeded in each Leighton tube and were grown to confluence for 6 days at 37°C and in the presence of 5% CO_2 in 3 ml Iscove's modified Dulbecco's medium, 10% fetal calf serum (FCS, Gibco BRL, England), and 1% penicillin/streptomycin. After removal of the growth medium, each monolayer (2.3×10^6 cells) was washed with 3 ml of Dulbecco's minimum essential medium (DMEM, Biochrom, Germany) containing 10% FCS and incubated in 3 ml of fresh DMEM for 1 h. During this time the cells which had grown in the presence of 23 mM glucose were equilibrated to 6 mM glucose of DMEM. Under these experimental conditions, the majority of HG cells were in G_0/G_1 -phase of the cell cycle (G_0/G_1 : $79.3 \pm 3.3\%$, G_2 : $9.8 \pm 2.4\%$, S: $11.2 \pm 1.7\%$). The doubling time of this cell line was about 36 h.

2.2 Calculation of $R_{\text{F/G}}$

For the measurement of ^{18}F FDG uptake the equilibration medium, DMEM, was replaced by 1 ml of fresh DMEM containing 10% FCS, 6 mM glucose, and 7.4 kBq (0.2 μCi) and ^{18}F FDG. ^{18}F FDG was produced at the Institute of Nuclear Chemistry of the Research Center Jülich (Hamacher *et al* 1986). The radioactivity of the medium of each sample was measured with a gamma-counter (Gammaszint model 5300, Berthold and Friesecke) at the beginning and at the end of 45 min incubation at 37°C with mild shaking (20 cycles min^{-1}). The difference of the two measurements after the correction of ^{18}F -decay was the loss of ^{18}F FDG from the extracellular medium

representing the utilization of ^{18}F FDG by 86HG-39 cells. The loss of extracellular glucose, monitored by hexokinase and 6-phosphate dehydrogenase assay using the auto-analyzer RA-X (Technicon, Bayer), represented glucose utilization. The $R_{\text{F/G}}$ was calculated using these two measurements.

2.3 Exposure of cells to γ -radiation

A ^{137}Cs -source (Gammacell 40, Atomic Energy of Canada Ltd.) was used for γ -irradiation (dose rate: 1.07 Gy min^{-1}).

2.3a Single fraction exposure to γ -radiation: Leighton tubes containing monolayers of 2.3×10^6 human glioblastoma cells were irradiated at room temperature with 1, 2, 8 or 16 Gy. The $R_{\text{F/G}}$ was determined 4, 12 or 24 h after termination of the γ -irradiation. The post-irradiation incubation was carried out at 37°C .

2.3b Single fraction versus multiple fractions exposure to γ -radiation: Leighton tubes with cell monolayers (see above) were irradiated at room temperature four times with 2 Gy each (multiple fraction). After each fraction of irradiation the tubes were left at 37°C for 12 h. These were compared with samples which were irradiated with 8 Gy γ -rays (single fraction) and left for 12 h at 37°C after irradiation.

Data points represent at least 5 independent experiments each comprising 3–5 replicates. The controls were sham-irradiated and kept under identical conditions as the irradiated samples.

2.4 Analysis of data

Data are given as mean \pm standard error of the mean (SEM). The significance of mean differences was evaluated using the paired and unpaired two sided *t*-test. Outliers were identified by the Nalimov-test (1972) and removed from the analysis. *P* values less than 0.05 were regarded as biologically significant.

3. Results

Figure 1 shows the $R_{\text{F/G}}$ as a function of a single fraction ^{137}Cs - γ -radiation dose of 1, 2, 8 or 16 Gy. The measurements of the $R_{\text{F/G}}$, performed at 4, 12 or 24 h after irradiation, have been separately shown. The radiation dose-response curve for the 4 h post-irradiation incubation did not show a significant influence of radiation on $R_{\text{F/G}}$. Different doses of radiation affected the $R_{\text{F/G}}$ when monitored after 12 and 24 h post-irradiation times. The curves revealed a significant increase of $R_{\text{F/G}}$ at 1 Gy (12 h: $P < 0.03$), 2 Gy (24 h: $P < 0.01$), and 8 Gy (12 h: $P < 0.03$; 24 h: $P < 0.01$).

Figure 2 shows the $R_{\text{F/G}}$ as a function of mode of

irradiation. Eight Gy radiation dose was administered either as a single fraction (SF) or as multiple fractions (MF) of 2 Gy each (4×2 Gy). The measurements of $R_{\text{F/G}}$ were carried out at 12 h post-irradiation time. Whereas $R_{\text{F/G}}$ increased significantly ($P < 0.01$) from the control level of 0.99 ± 0.02 (figure 2A₁) to 1.23 ± 0.05 (figure 2A₂) after SF, it decreased significantly ($P < 0.02$) to 0.86 ± 0.03 after MF (figure 2A₃). Figure 2B shows the individual values of the ^{18}F FDG utilization and that of the glucose under conditions described in figure 2A.

4. Discussion

In this study the $R_{\text{F/G}}$ has been measured in a simplified *in vitro* model. The fractional extraction of the tracer ^{18}F FDG and that of 6 mM glucose from the extracellular medium in 45 min represents utilization of these molecules by the monolayer cells in a steady state. Fractions of ^{18}F FDG and glucose taken up by the cells might be metabolized in the period of assay spreading over 45 min. Whereas it has been reported for rat and for normal human brain that the entrapped ^{18}F FDG and glucose are not likely to be metabolized in this period, nothing is known with certainty for tumour cells (Schmidt *et al* 1996). Since cancerous cells are known to have higher rate of glucose metabolism and the glioblastoma cell line used in this study is a transformed cell line, the

assay had to ensure that no erroneous values are measured. By counting ^{18}F FDG after washing the cells or by assaying intracellular glucose after 45 min, the loss of ^{18}F FDG or glucose due to metabolism could not be accounted for. Therefore, the strategy for measuring the utilization of ^{18}F FDG and of glucose was changed in this study. The measure of loss of extracellular ^{18}F FDG and glucose from the medium in 45 min, as performed in this study, represents total uptake and metabolism of ^{18}F FDG and glucose by cells during this time.

To find out the appropriate condition even for the simplified *in vitro* model, the time of post-irradiation incubation has been verified (figure 1). Measurements done after 12 or 24 h following irradiation resulted in statistically significant increase of $R_{\text{F/G}}$ at different doses as compared with the controls. In line with common clinical practice of 12 hourly irradiation of patients in a fractionated dose protocol, 12 h post-irradiation time was selected in this piece of work to measure $R_{\text{F/G}}$ after SF and MF modes of irradiation.

The $R_{\text{F/G}}$ of unperturbed monolayer cells was found to be 0.99 ± 0.02 (figures 1 and 2A₁) indicating that the *in vitro* uptakes of ^{18}F FDG and glucose were nearly identical. This is quite different from the reported LC values (0.4–0.5) in most brain regions under normal *in vivo* conditions (Gjedde *et al* 1985). The *in vitro* and

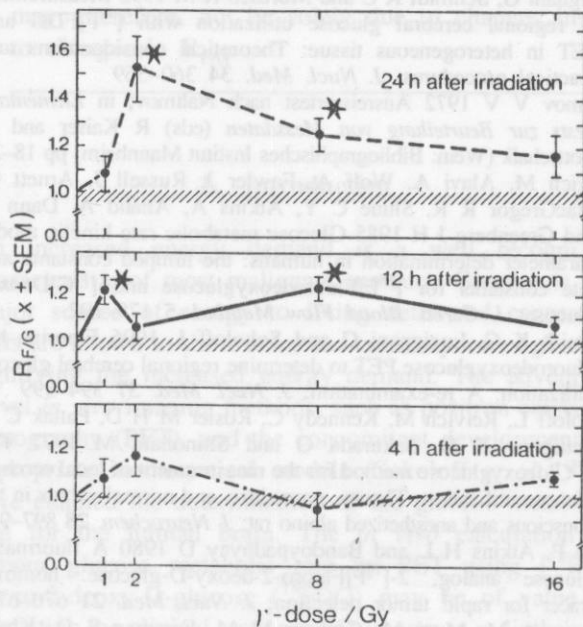


Figure 1. Changes in the $R_{\text{F/G}}$ as a function of single fraction ^{137}Cs - γ -irradiation measured at different post-irradiation times. The shaded areas represent the mean $R_{\text{F/G}}$ (SEM of 95 non-irradiated monolayer cultures (0.99 ± 0.02)) kept under otherwise identical conditions. The radiation induced $R_{\text{F/G}}$ which are significantly different to the controls are marked by (*).

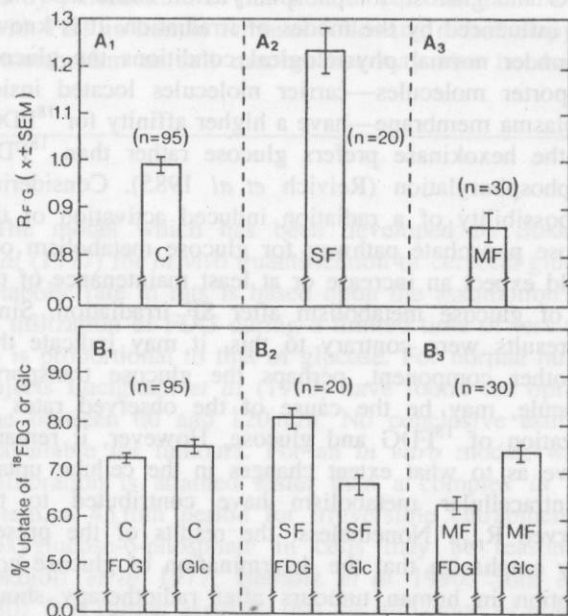


Figure 2. $R_{\text{F/G}}$ of non-irradiated control (C) cells (top panel A₁), of cells irradiated to 8 Gy in a single fraction (SF) (top panel A₂) and of cells irradiated to 4×2 Gy in a schedule of multiple fractions (MF) (top panel A₃). These values were calculated from the measurements of per cent of ^{18}F FDG-over per cent of glucose uptakes by cells from the medium (shown in the bottom panel B₁, B₂ and B₃). All measurements were made at 12 h post-irradiation time.

in vivo situations are different due to organizational difference between 2-dimensional cell monolayer and 3-dimensional tissue, and the physiological difference due to vascularization of tissue which is absent in a cell monolayer. Nonetheless, the $R_{F/G}$ data reported here look similar to the *in vivo* LC values reported by Kapoor *et al* (1989). This seems to support the assumption that $R_{F/G}$ *in vitro* corresponds to the LC *in vivo*.

The *in vitro* study reveals that the $R_{F/G}$ varies with the dose and the mode of γ -irradiation. The radiation induced changes of $R_{F/G}$ (figures 1 and 2) are comparable to the reported LC of four patients with malignant cerebral gliomas, where the LC varied between 0.38 and 0.70 before radiotherapy and between 0.53 and 1.13 after radiotherapy (Spence *et al* 1995). Considering differential uptake of ^{18}F FDG and glucose after irradiation (figure 2B), it is interesting to note that the increase of the $R_{F/G}$ after a SF irradiation is due to an increase of ^{18}F FDG uptake and a decrease of glucose uptake. After MF irradiation, the decrease of $R_{F/G}$ (figure 2A₃) was primarily due to the lower ^{18}F FDG uptake (figure 2B₃). This demonstrates that FDG uptake may vary independently of the glucose metabolism indicating that a change in the uptake of FDG after exposure to radiation may not reflect true status of glucose metabolism.

The analysis of the results (figure 2B) suggests that the mode of irradiation influenced the kinetics of ^{18}F FDG as well as glucose uptake. The different affinities of ^{18}F FDG and glucose for phosphorylation could also have been influenced by the modes of irradiation. It is known that under normal physiological conditions the glucose transporter molecules—carrier molecules located inside the plasma membrane—have a higher affinity for ^{18}F FDG, and the hexokinase prefers glucose rather than ^{18}F FDG for phosphorylation (Reivich *et al* 1985). Considering the possibility of a radiation induced activation of the pentose phosphate pathway for glucose metabolism one should expect an increase or at least maintenance of the rate of glucose metabolism after SF irradiation. Since our results were contrary to this, it may indicate that the other component, perhaps the glucose transporter molecule, may be the cause of the observed rates of utilization of ^{18}F FDG and glucose. However, it remains elusive as to what extent changes in the cellular uptake or intracellular metabolism have contributed to the observed $R_{F/G}$. Nonetheless, the results of the present study emphasize that the determination of glucose consumption in human tumours after radiotherapy should be done with caution. This will probably also apply to chemotherapy (Langen *et al* 1989). Even in a full kinetic modelling approach using a measurement of cerebral blood volume and fitting of individual rate constant of tracer, variations of the $R_{F/G}$ may significantly influence

the result of the calculated value of glucose consumption for clinical use.

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